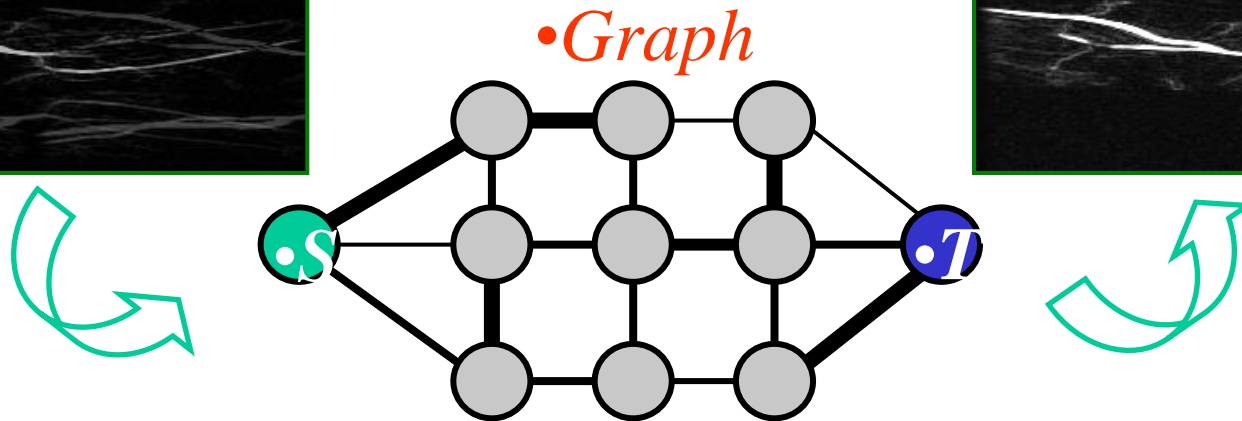
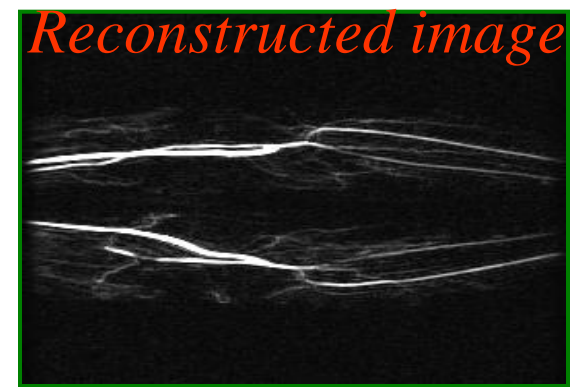
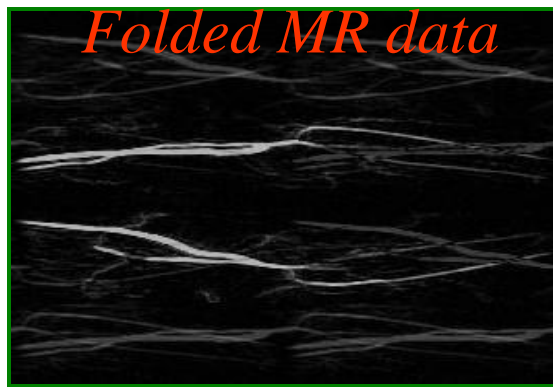


Recon Core subproject III

MRI Reconstruction Using Graph Cuts:

Ashish Raj, Weill Cornell Medical College New York

- *A new graph-based algorithm **
- *Inspired by advanced robotic vision, computer science*



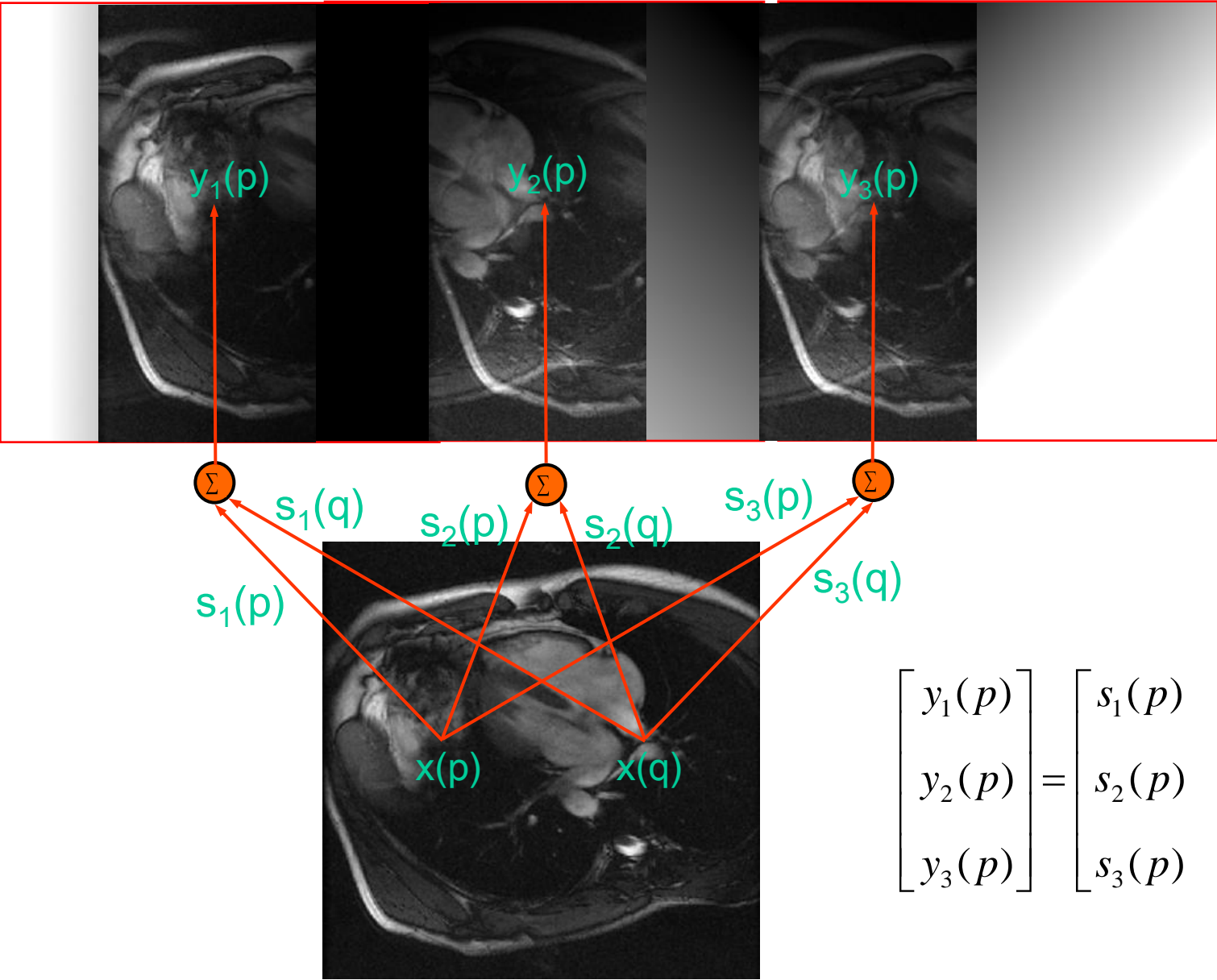
- *Operations on this graph produce reconstructed image!*

- *Raj et al, Magnetic Resonance in Medicine, Jan 2007,*
- *Raj et al, Computer Vision and Pattern Recognition, 2006*
- *Singh et al., MRM (to appear)*

Project Summary

- Aim1: To apply EPIGRAM to fast high-resolution structural brain imaging
 - Image priors to be empirically evaluated
- Aim 2: Extending the method from 2D to 2D + time data
- Aim 3: Validation
- Aim 4: Developing new efficient, feasible Graph algorithms

Significant advances were made in all aims (except Aim 3)



$$\begin{bmatrix} y_1(p) \\ y_2(p) \\ y_3(p) \end{bmatrix} = \begin{bmatrix} s_1(p) & s_1(q) \\ s_2(p) & s_2(q) \\ s_3(p) & s_3(q) \end{bmatrix} \begin{bmatrix} x(p) \\ x(q) \end{bmatrix}$$

Least squares solution

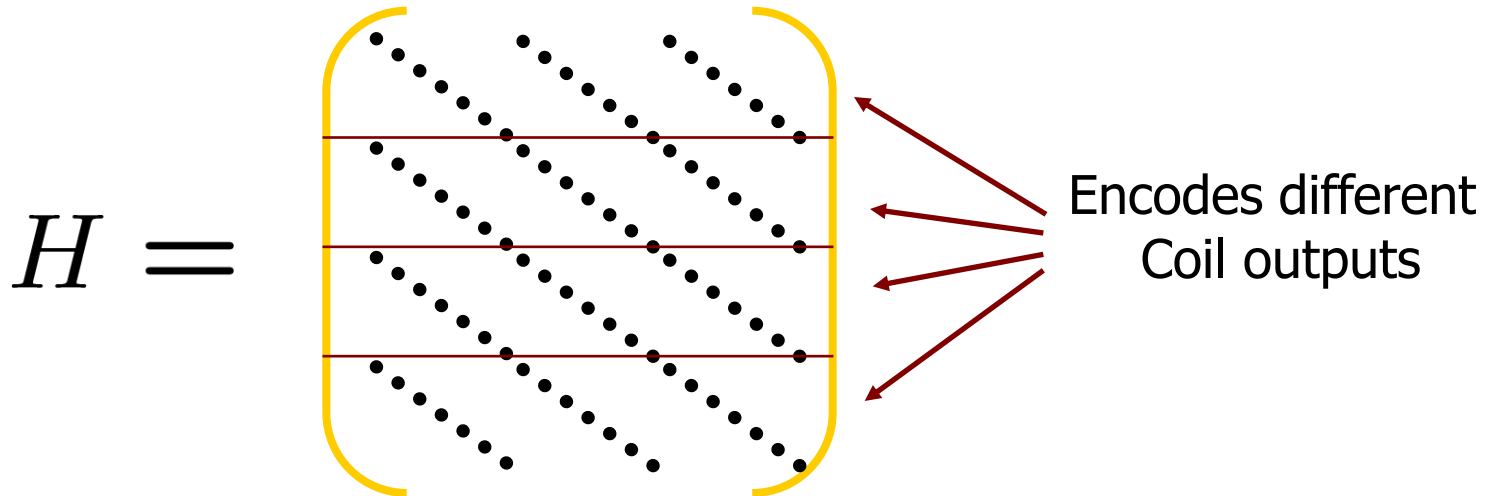
- Least squares estimate:

$$(\hat{x}(p), \hat{x}(q)) = \arg \min_{x(p), x(q)} \sum_{l \in \text{Coils}} [y_l(p) - s_l(p)x(p) - s_l(q)x(q)]^2$$

– Famous MR algorithm: SENSE (1999)

- Linear system

$$y = Hx + n$$



EPIGRAM Summary

- Finds the MAP estimate

$$\hat{x} = \arg \min_x E(x) \equiv \left[\|y - Hx\|^2 + \lambda G(x) \right]$$

Makes Hx close to y

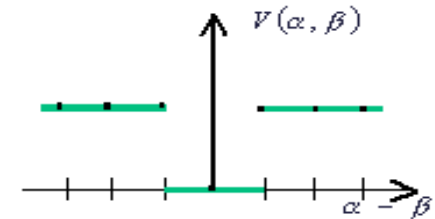
Makes x piecewise smooth

- Used Markov Random Field priors

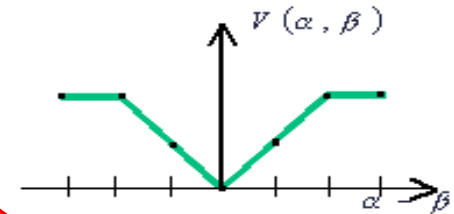
$$G(x) = \sum_{(p,q) \in \mathcal{N}} V(x_p - x_q)$$

- If V “levels off”, this preserves edges

Potts function



Truncated L1 distance



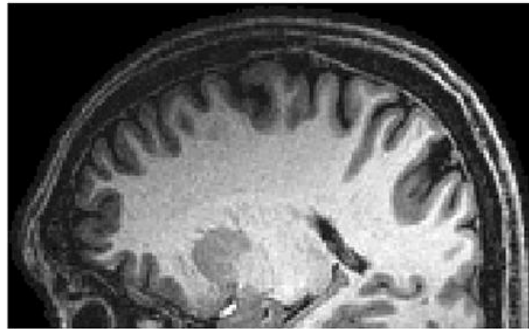
Robust

New Developments (I):

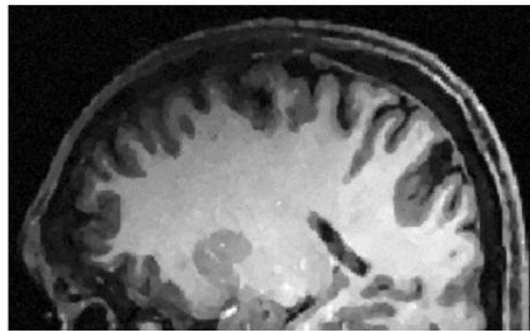
- Extension of EPIGRAM from 2D to 3D
- Phase-constrained reconstruction

Phase Constrained EPIGRAM: $R_{\text{eff}} = 4.5$

Reference:
Sum of squares

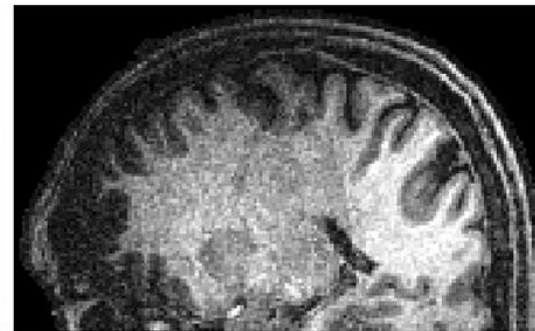


(a)



(b)

Fast EPIGRAM



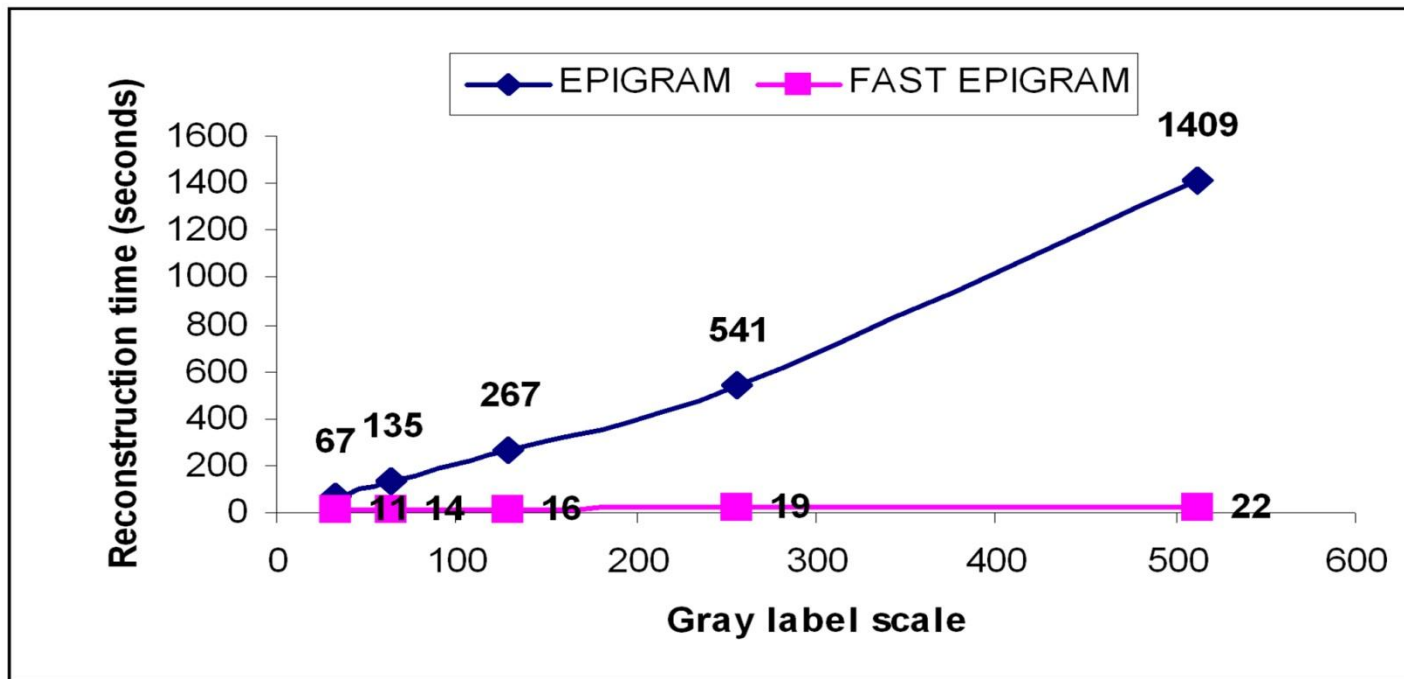
(c)

Regularized SENSE

New Developments (II):

- Fast EPIGRAM – uses “jump moves” rather than “expansion moves”
 - Up to 50 times faster!

New, Faster Graph Cut Algorithm: Jump Moves

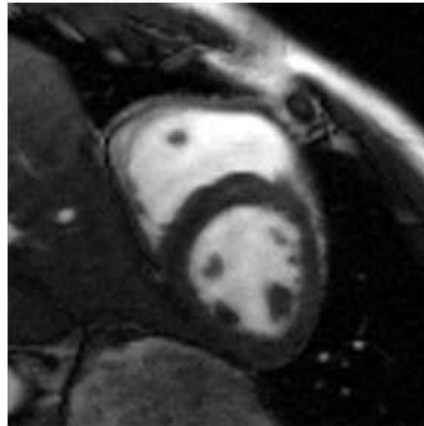


- *Reconstruction time of EPIGRAM (alpha expansion) vs Fast EPIGRAM (jump move)*
 - after 5 iterations over [32, 64, 128, 256, 512] gray scale labels
 - image size 108x108 pixels.
- *Linear versus exponential growth in reconstruction time*

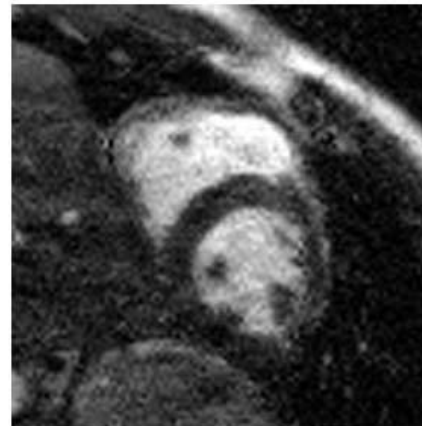
Jump Move Results: Cardiac Imaging, R=4

- *reconstruction for cine SSFP at $R = 4$*

Reference:
Sum of squares



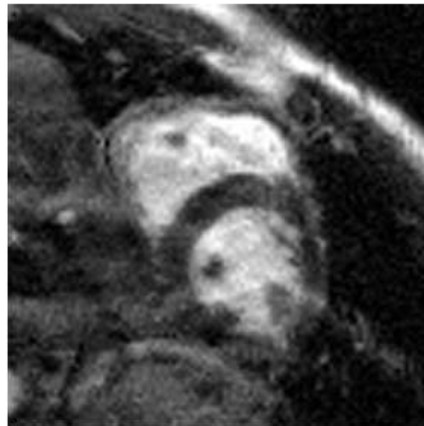
(a)



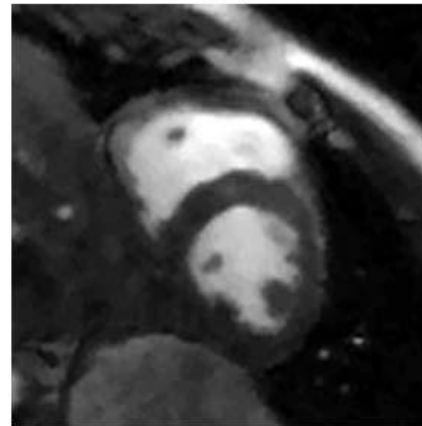
(b)

Regularized SENSE
($\mu = 0.1$)

Regularized SENSE
($\mu = 0.5$)



(c)



(d)

Fast EPIGRAM

New Developments (III):

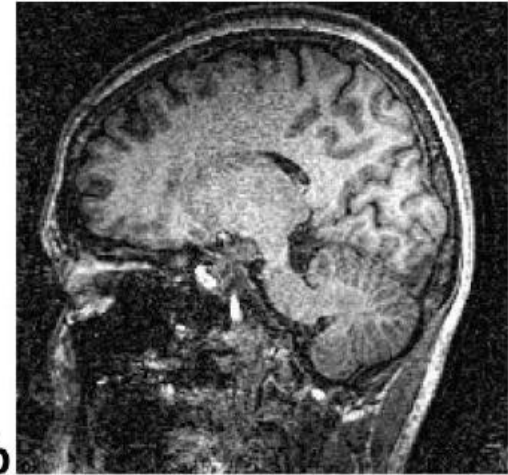
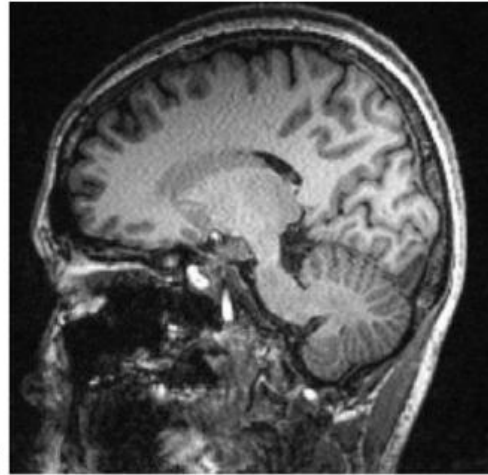
Automatically Learning Image Priors

- The most important aspect of EPIGRAM is choice of prior
- What is the most appropriate prior model?
- Recon performance depends crucially on prior model
- Recall:

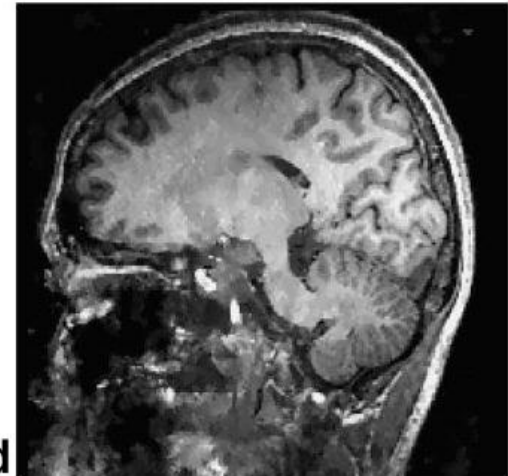
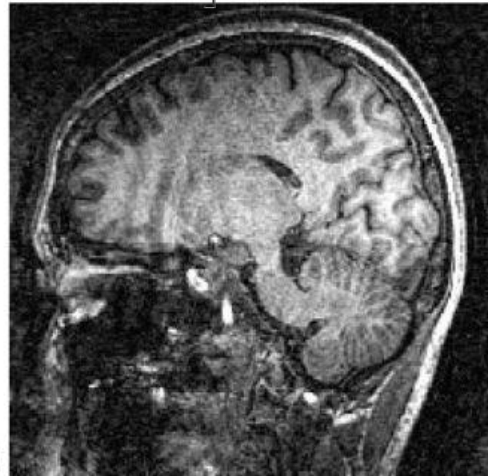
$$\hat{x} = \arg \min_x E(x) \equiv \left[\|y - Hx\|^2 + \lambda G(x) \right]$$

$$G(x) = \sum_{(p,q) \in \mathcal{N}} V(x_p - x_q)$$

*Form of V
determines
recon image*



$$V(\delta) = 0.1|\delta|^2$$



$$V(\delta) = 0.2|\delta|^2$$

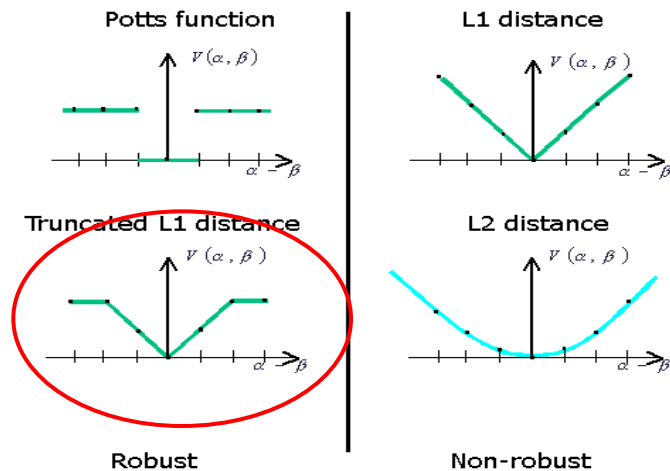
$$V(\delta) = 0.1 \min(50, |\delta|)$$

New Developments (III):

Automatically Learning Image Priors

- New idea: automatically learning what prior model best fits brain MRI
- Generalization of edge-preserving Gibbs priors successful in EPIGRAM
- Define a class of prior distributions → mixture of various powers

$$G(x) = \sum_{(p,q) \in \mathcal{N}} V(x_p - x_q)$$



Original prior model

image $\delta = x_1 - x_2$ *Diff image*

$$Pr(x) = Pr(\delta) \propto \exp \left(-\frac{1}{2M} \sum_{\delta} V_{\gamma, \alpha, K}(\delta) \right)$$

$$V_{\gamma, \alpha, K} = \sum_{i \in \gamma} \frac{\alpha_i \min(\delta^{p_i}, K_i^{p_i})}{p_i}$$

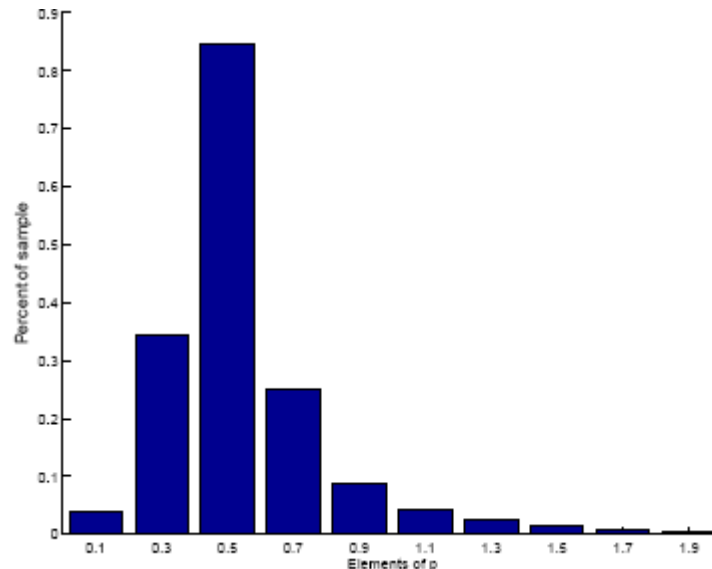
exponent *Mixture weight* *cutoff*

Proposed prior model

Learning Image Priors: Technique

- Used Markov chain Monte Carlo (McMC) technique to learn unknown parameters of prior model
- McMC sampling is based on Metropolis-Hastings algorithm
- After 1000s of iterations, gives a posterior distribution of the model
- We use the maximum of this inferred posterior

Histogram of various exponents “visited” by McMC sampler



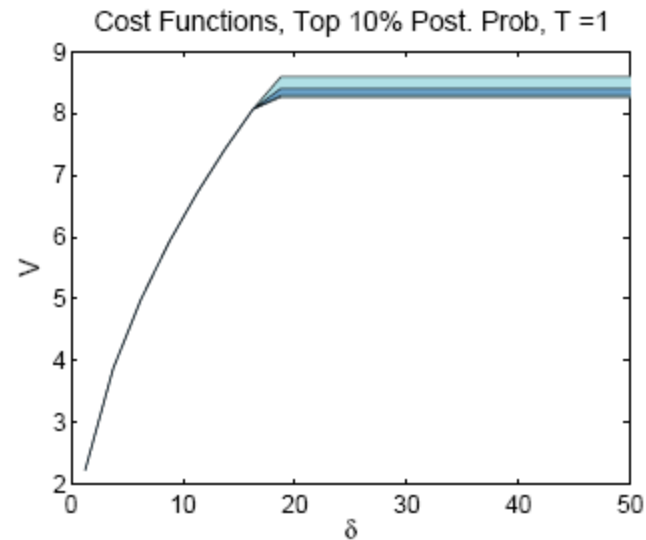
Learning Image Priors: Results

- Found a strong maximum of posterior
- Inferred model: exponent = 0.5, cutoff = 25

$$V_{\gamma, \alpha, K} = \min(\delta, 25.42)^{0.5}$$

exponent

cutoff



We believe this prior will be superior to previous prior
Results on brain data awaited

Learning Image Priors: Simulations

- Shepp-Logan head phantom with different noise and blur (PSF)
- Width of Gaussian blur kernel: 0, 2, 4, 6, 8, 10, 20
- Inferred model should depend on size of blur
 - (more blurry image \rightarrow higher exponent)

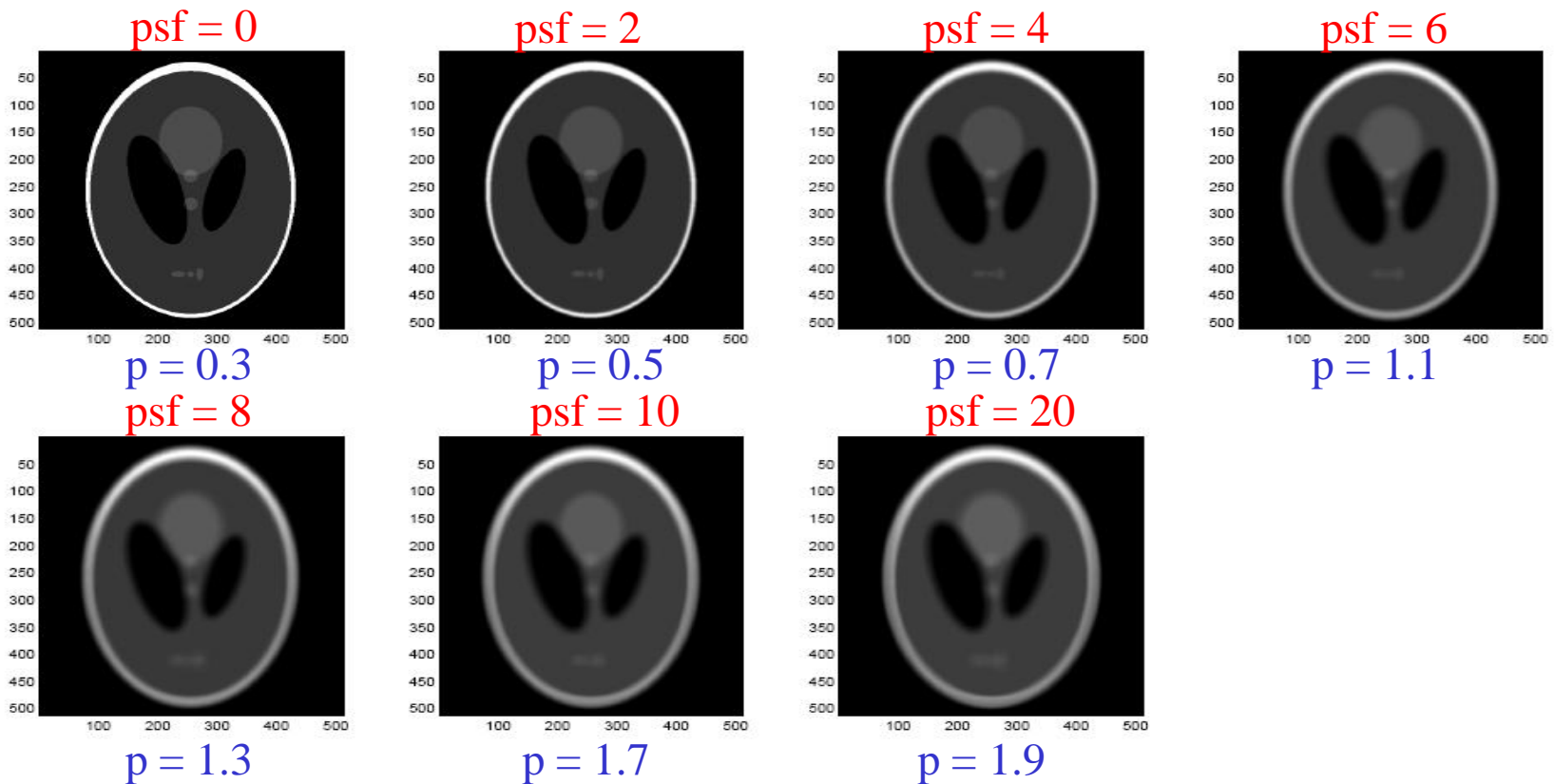


Figure 1: The different images corresponding to the different widths of Gaussian blur.

Learning Image Priors: Simulations

Result: found almost linear dependency

Blur Width	Parallel Tempering, $T = 1$	Regular Sampling, $T = 1$
0	$\min(\delta, 57.70)^{0.3}$	$\min(\delta, 55.67)^{0.3}$
2	$\min(\delta, 17.57)^{0.5}$	$\min(\delta, 16.56)^{0.5}$
4	$\min(\delta, 7.79)^{0.7}$	$\min(\delta, 7.77)^{0.7}$
6	$\min(\delta, 4.46)^{1.1}$	$\min(\delta, 4.47)^{0.9}$
8	$\min(\delta, 3.14)^{1.3}$	$\min(\delta, 3.07)^{1.3}$
10	$\min(\delta, 2.24)^{1.7}$	$\min(\delta, 2.21)^{1.7}$
20	$\min(\delta, 1.93)^{1.9}$	$\min(\delta, 1.91)^{1.9}$
Brain MRI	$\min(\delta, 11)^{0.5}$	$\min(\delta, 11.67)^{0.5}$

Table 1: The estimate of the MAP for the 7 different blurred Shepp-Logan Phantoms, as well as brain MR images.

New Developments (IV):

- New graph cut algorithm to replace EPIGRAM – does not use expansion moves at all
- Expect $o(10-100\times)$ computational speed up
- Based on exploring null-space of system matrix H

$$E(x) \equiv \left[\|y - Hx\|^2 + \lambda G(x) \right]$$

- Let $D = \text{null}(H)$, x_0 be any solution to $y = Hx$
- Let $x = x_0 + D\eta$. Then $y - Hx = y - Hx_0$ and $E(x) = \lambda G(\eta)$
- Henceforth we seek graph cut moves on η rather than x
- Since nullspace is much smaller than space of x , this is much more efficient